

Statistical Physics Approaches to High-Dimensional Inference

applications to biological data

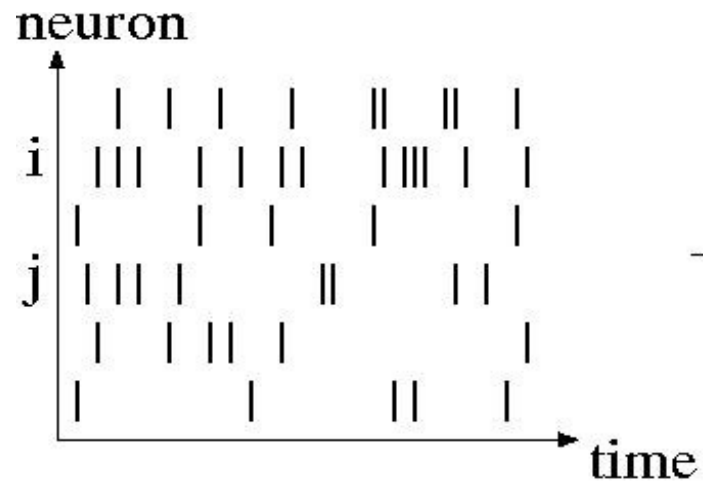
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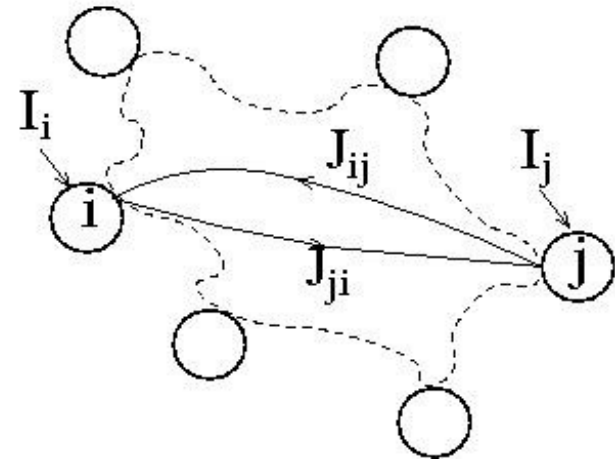
Winter School on Quantitative Biology, ICTP, December 2012

- Monday: Theoretical framework for model inference
(special case: many interacting & stationary variables)
Mean-field inference
Applications covariation in protein families (I)
- Yesterday: Issues & advanced statistical physics methods
Inverse Hopfield model & Random Matrix Theory
Applications to covariation in proteins (II)
to neural data (I)
- **Today:** Case of interacting & non-stationary variables
Applications to neural data (II)

Getting functional interactions from the activity



?



Data (spiking times)

Functional Interactions

Approaches

- Principal Component Analysis or Independent Component Analysis
- Granger Causality (regressive models)

- Stationary Models:

Maximum Entropy Models

- Dynamical Models:

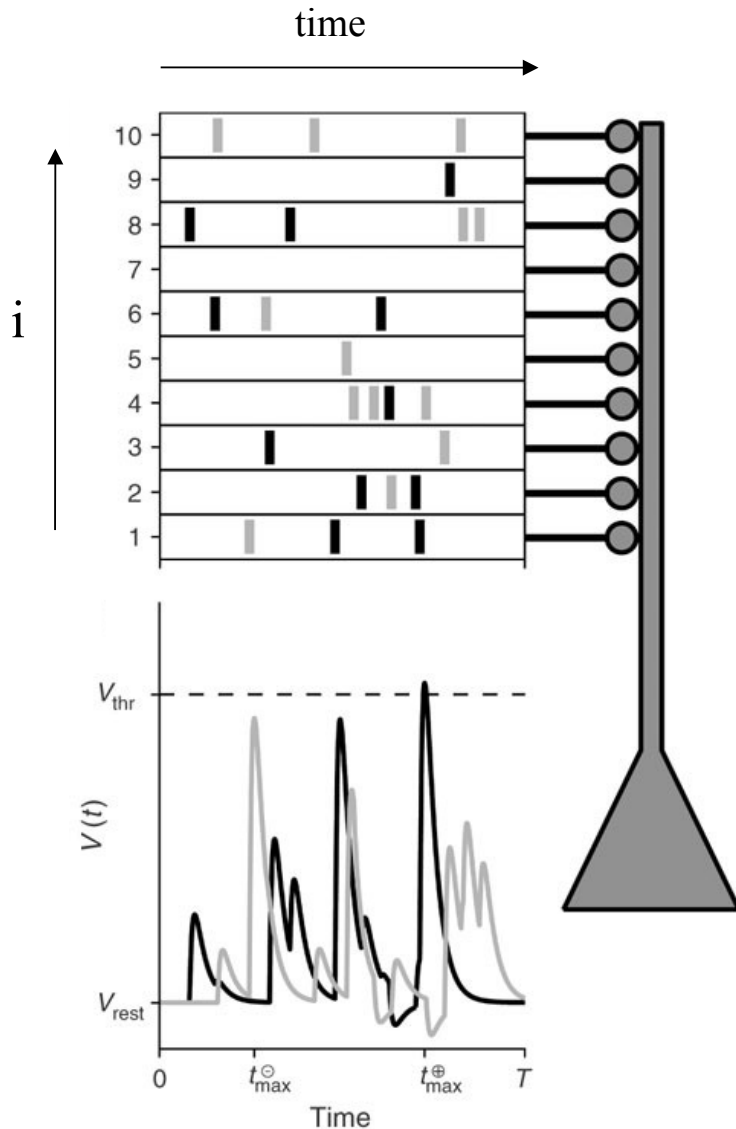
Generalized Linear Models

Integrate-and-Fire Models



**Bayesian
approaches**

The Leaky Integrate-&-Fire model



$$C \frac{dV}{dt}(t) = -g V(t) + \sum_i J_i \sum_n K(t-t_{i,n}) + \eta(t)$$

+ comparison with threshold

active

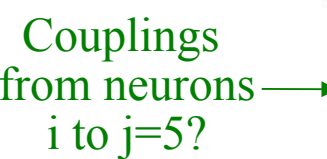


or

silent

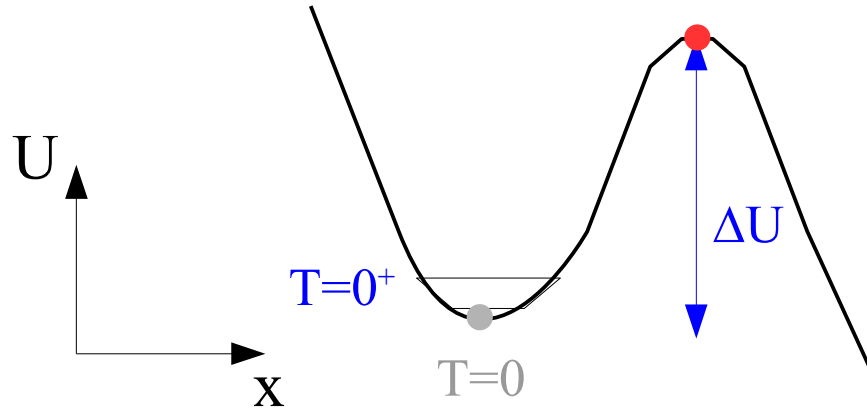


Inference of Synaptic Weights from Raster Plots

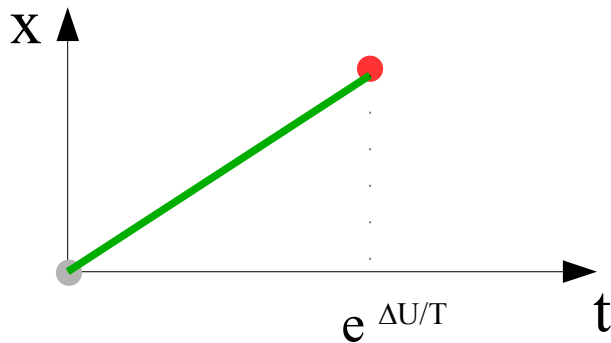


- (Paninski et al., 2004)]

Optimal Paths for the Potential and the Noise (1)



Small T:

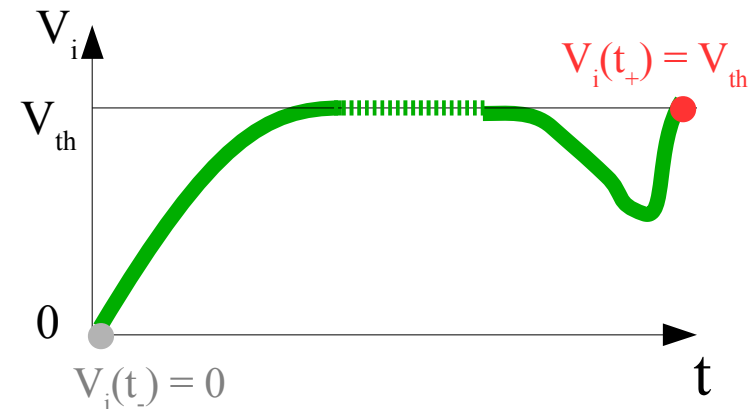


U defines the optimal paths for $x(t)$ and $f(t)$

(Langer 1967)

Small σ :

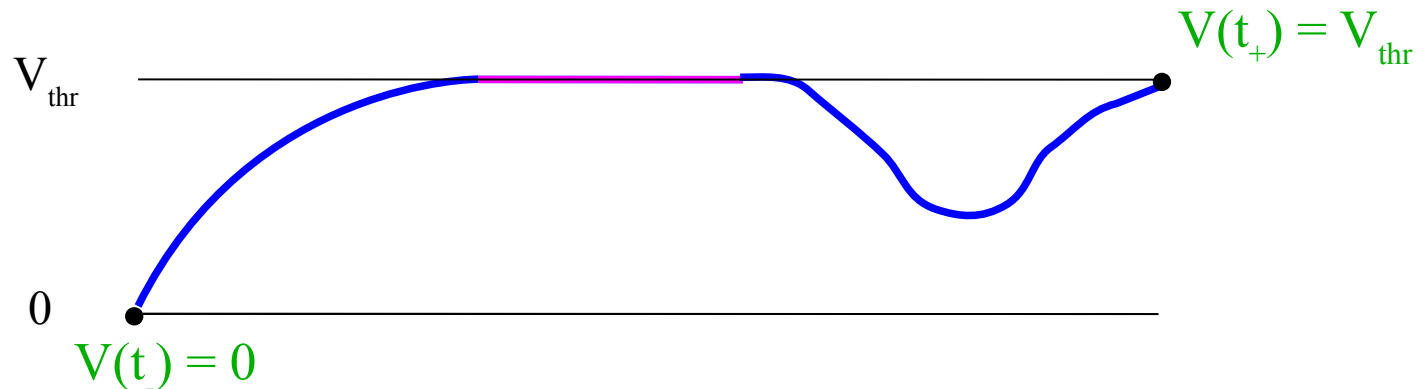
The likelihood P , given $J, I, \{t_{j,k}\}$, defines the optimal paths for the potential V_i and the noise (current) η_i



— or — ?

Optimal Paths for the Potential and the Noise (2)

Small σ : The likelihood P , given $J, I, \{t_{j,k}\}$, defines the optimal paths for the potential V_i and the noise (current) η_i



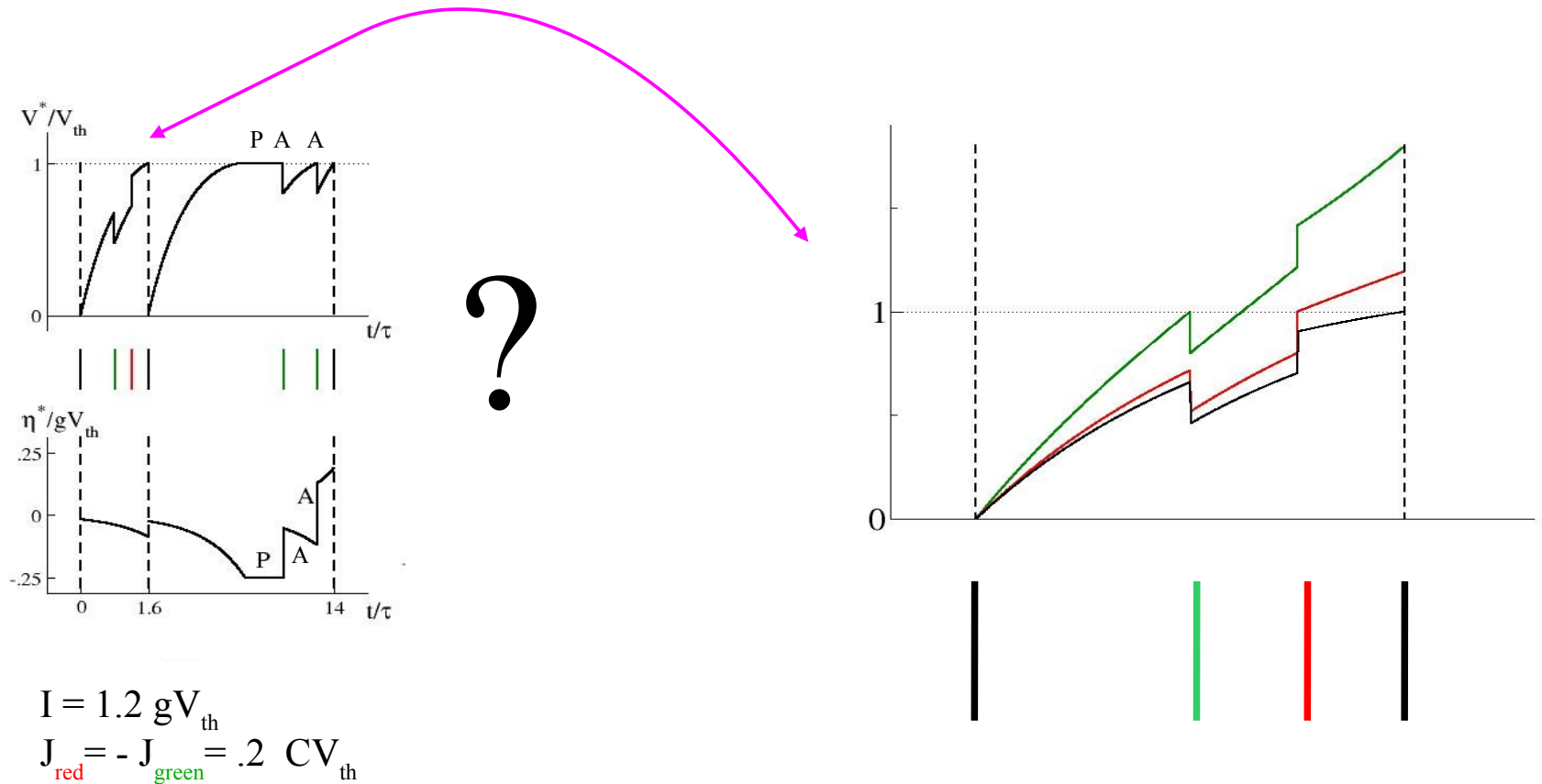
$$\left. \begin{aligned} \frac{dV}{dt}(t) &= -g V(t) + \sum_i J_i \sum_n K(t-t_{i,n}) + \eta(t) \\ \frac{d\eta}{dt}(t) &= +g \eta(t) \end{aligned} \right\} \text{ or } \left\{ \begin{aligned} V(t) &= V_{thr} \\ \eta(t) &= g V_{thr} - \sum_i J_i \sum_n K(t-t_{i,n}) \end{aligned} \right.$$

Particular case: $K = \delta$, i.e. instantaneous synaptic integration

S. Cocco, S. Leibler, R.M. (2009); R.M., S. Cocco (2011)

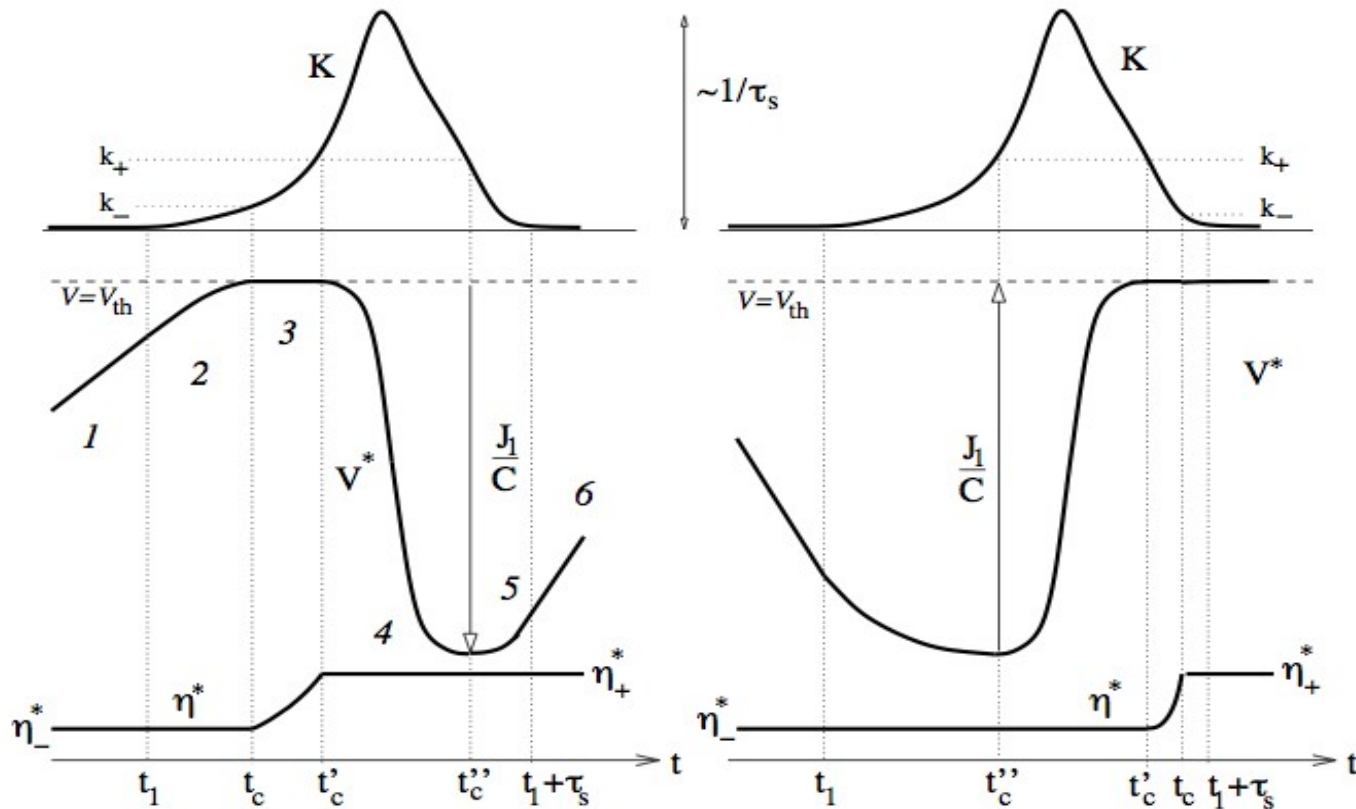
Looking for Contacts (1)

Simplest case : no intermediate contact with the threshold potential



Looking for Contacts (2)

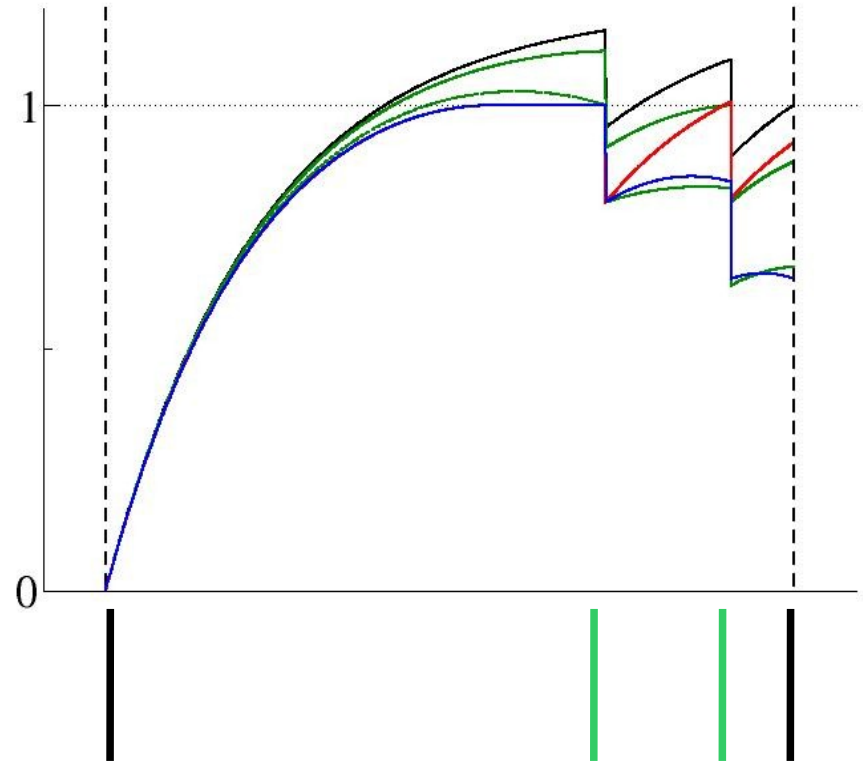
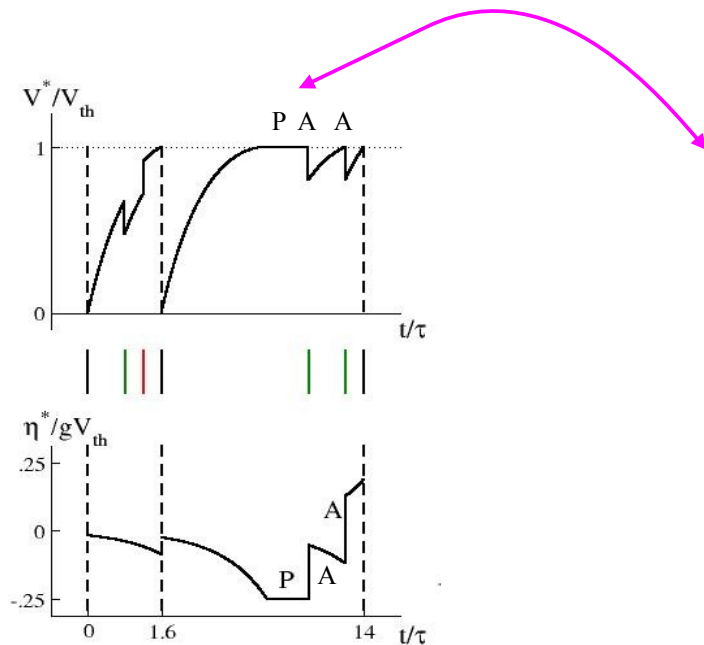
Analysis of the intermediate contact region :



Contact Rules: Contacts take place :

- Simultaneously to an input spike, with a discontinuous increase of the noise (**active contacts**)
- On a finite duration interval, during which noise is constant (**passive contacts**)

Looking for Contacts (3)

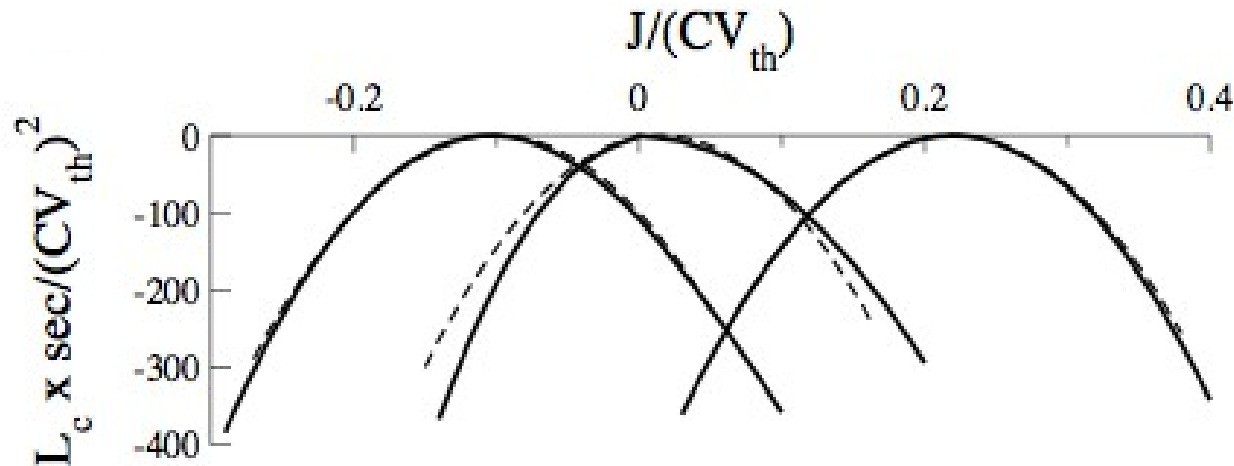


Practice:

- if the current and the interactions are known, the optimal paths for the potentials, for the noises, and the likelihood can be found in time = cst $N^2 \times S$
- optimal current and couplings are found by maximizing the likelihood (which is convex)

Properties of the inference procedure (1)

- Gives most likely interactions J and error bars ΔJ



- Tested on synthetic data generated from networks with known couplings; accurate as long as the noise variance is moderate: $\sigma^2 < f(g, C, V_{th}, ISI)$

Properties of the inference procedure (2)

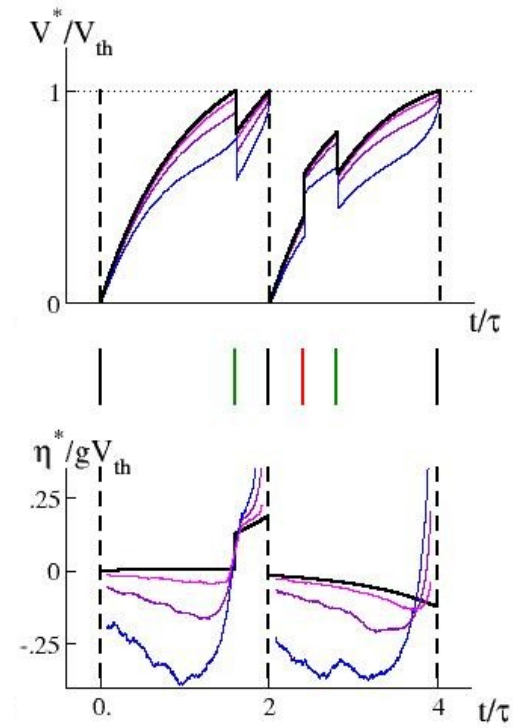
- Fast : recordings of 40 neurons, 170,000 spikes in 30 sec on commercial PC
(up to $N=160$, 5 millions spikes with synthetic data)

related works: $N=1$ neuron, ~ 100 spikes (for any σ) (Pillow et al., 2005)
 $N=5$ neurons, ~ 500 spikes ($\sigma=0$) (Maretsos et al., 2004)
time discretization \rightarrow constrained optimization (Koyama, Paninski, 2009)
- Limitations: synaptic integration kernel is instantaneous
no external stimulus so far
noise must be small (empirical extension to moderate noise)

How to deal with moderate noise? (1)

- optimal paths are exact in the $\sigma \rightarrow 0$ limit

- $\sigma = .07, .18, .36 \ V_{th} (g C)^{1/2}$
 $I = 1.2 \ g V_{th}, J_{red} = -J_{green} = .2 \ C V_{th}$



B

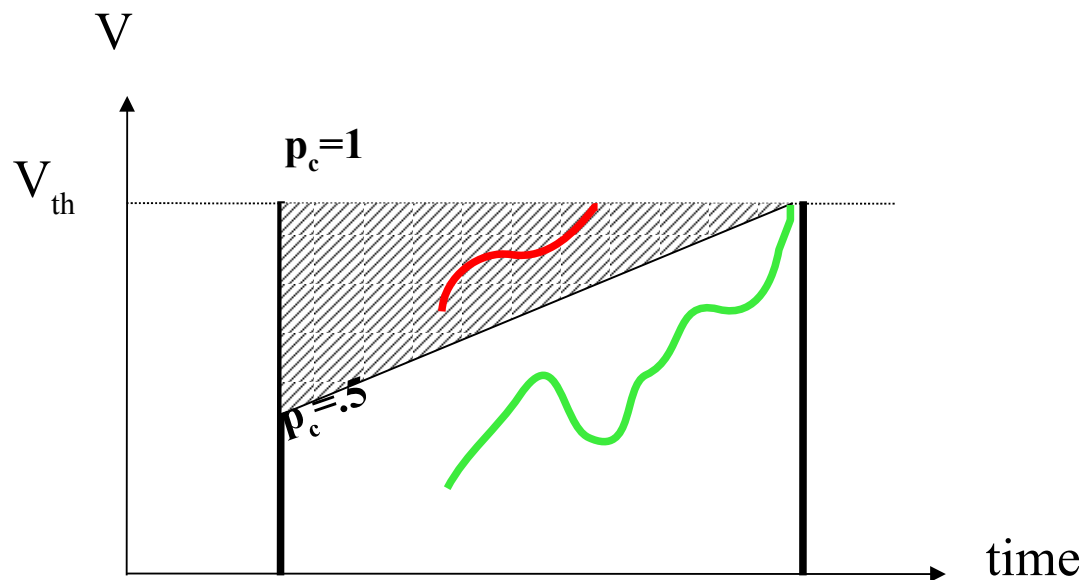
- Gaussian fluctuations around the $\sigma=0$ optimal path

$$\frac{\langle (V_i - V_i^*)^2 \rangle}{V_{th}^2} = \bar{\sigma}^2 \tanh\left(\frac{t_{i,k+1} - t_{i,k}}{2\tau}\right) \quad \text{with} \quad \bar{\sigma} = \frac{\sigma}{V_{th} \sqrt{gC}}$$

- Pessimistic point of view: Gaussian corrections to log-likelihood are independent of interaction parameters!

How to deal with moderate noise? (2)

- Probability of early crossing

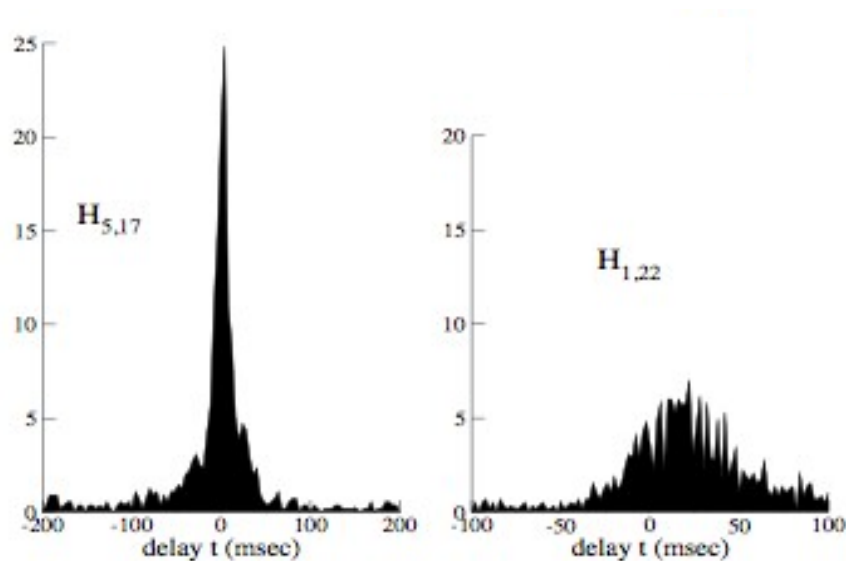


- Algorithm with Moving threshold $V_{th}(t)$...

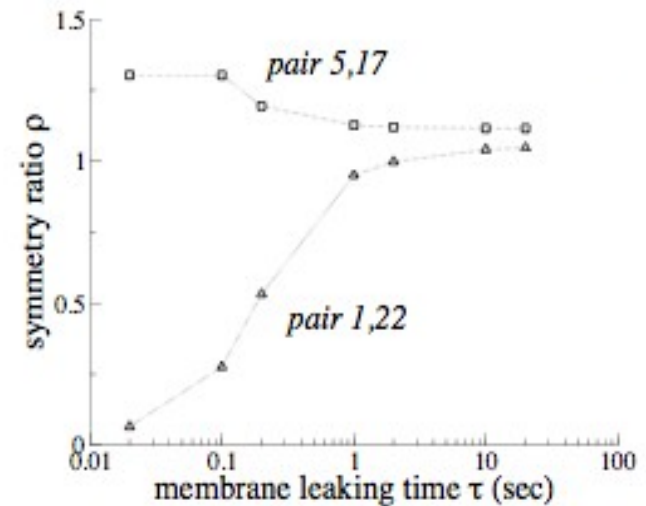
Application to Multi-Electrode Recordings (1)

*Asymmetry of interactions and time-scales
(spontaneous activity)*

Cross-correlograms



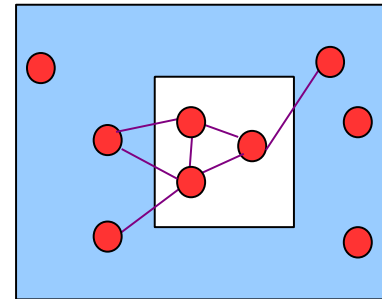
Ratio J_{ij} / J_{ji}



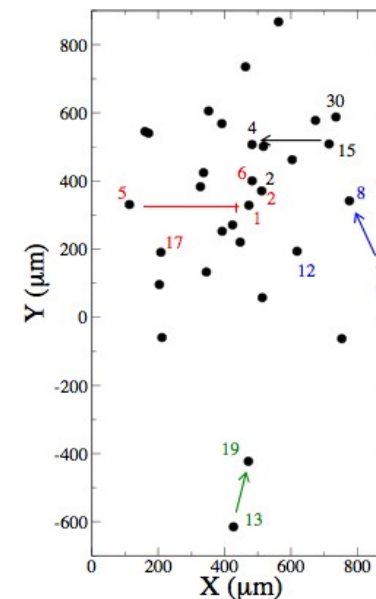
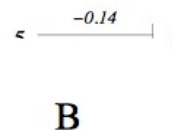
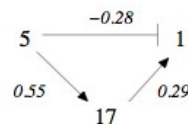
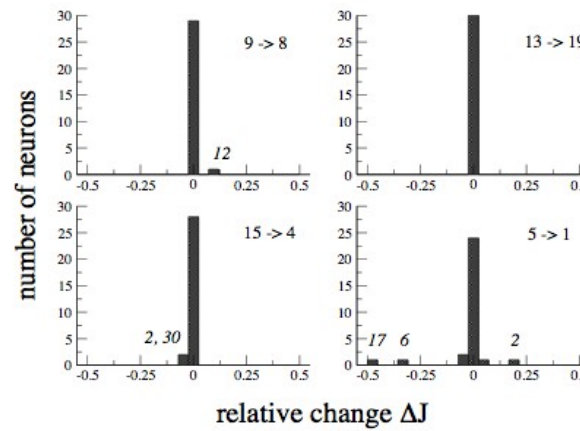
Application to Multi-Electrode Recordings (2)

Salamander retinal ganglion cell activity: (N=32 cells, spontaneous activity and random flickers - M. Meister)

Is the inference problem well-behaved?

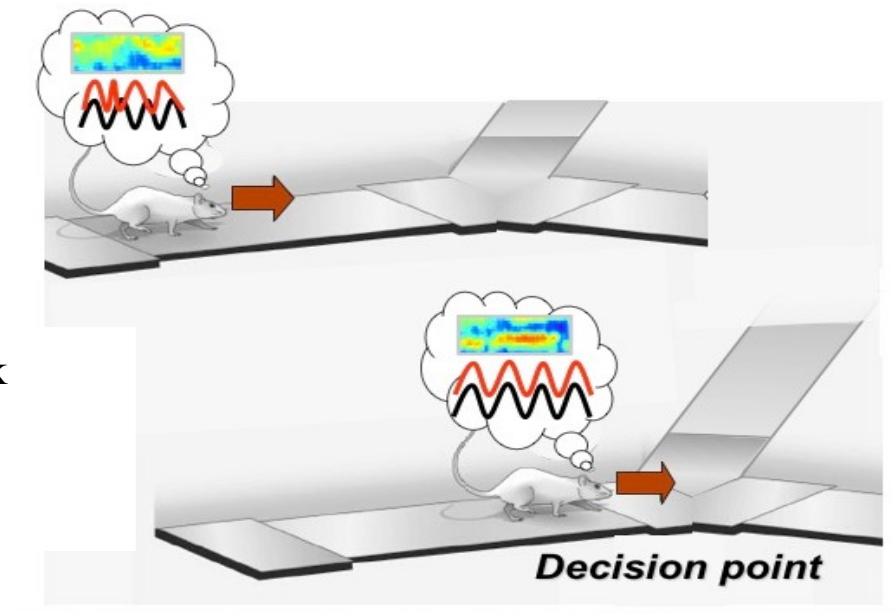


Spontaneous activity



Exploring learning and memory from in vivo cortical multi-electrode recordings

Peyrache, Battaglia et al. (2009): 37 cells
in prefrontal cortex, before, during and after a task



Principal component analysis of cortical recordings (Peyrache, Battaglia et al. 2008)

Rat perform a rule shift task four possible rules

Activity of prefrontal cortex is recorded during:

The sleep period prior the task (PRE)- the task- and the sleep period after the task (POST)

Patterns:

Starting with D. Hebb's (1949) theorists have postulated cell assemblies as the main unit of information representation which create a coherent input to downstream areas.

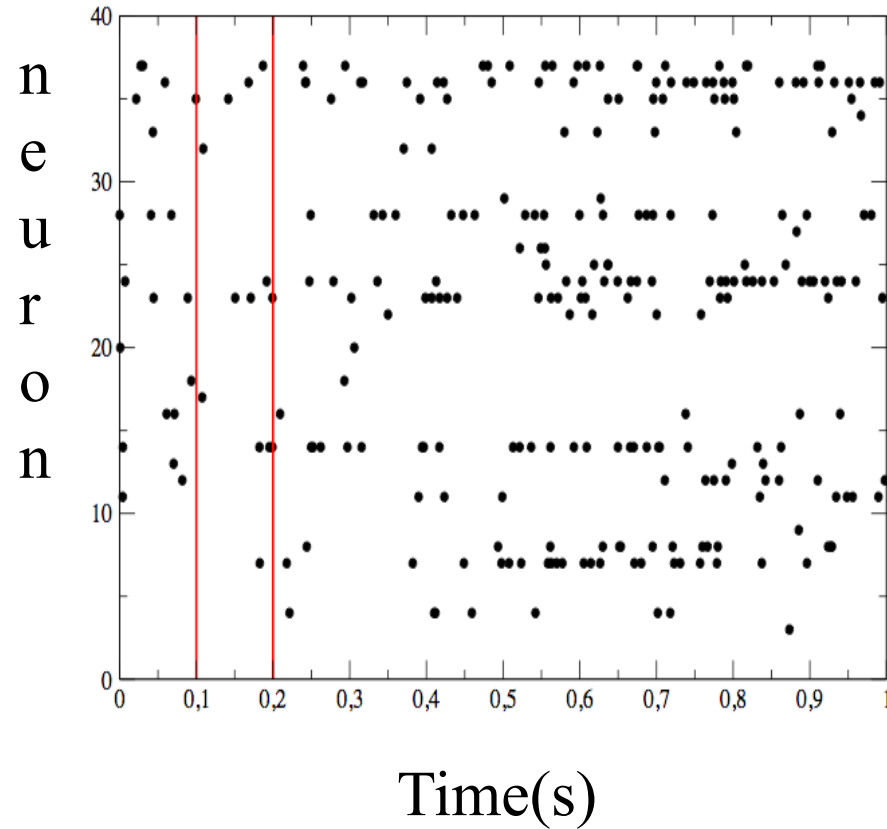
Replay and memory consolidation:

replay of the pattern of activity during the SWS (slow wave sleep) in period corresponding to coordinated bursts of activity of the hippocampus (sharp waves)

Replay of rule-learning related neural patterns in the prefrontal cortex during sleep A. Peyrache.. F. Battaglia Nature Neuroscience 2008,

Principal component analysis of ensemble recordings reveals cell assemblies at high temporal resolution A. Peyrache ... F. Battaglia J. Comput Neurosci 2009

1. Spike trains from the awake epoch are binned



Time is discretized in time windows of size $\Delta t = 100$ ms

$$s_i^\tau = \begin{cases} 1 & \text{if at least one spike in time window } k \\ 0 & \text{if no spike in time windows } k \end{cases}$$

$$p_{kl} = \frac{1}{B} \sum_{\tau=1}^B s_k^\tau s_l^\tau,$$

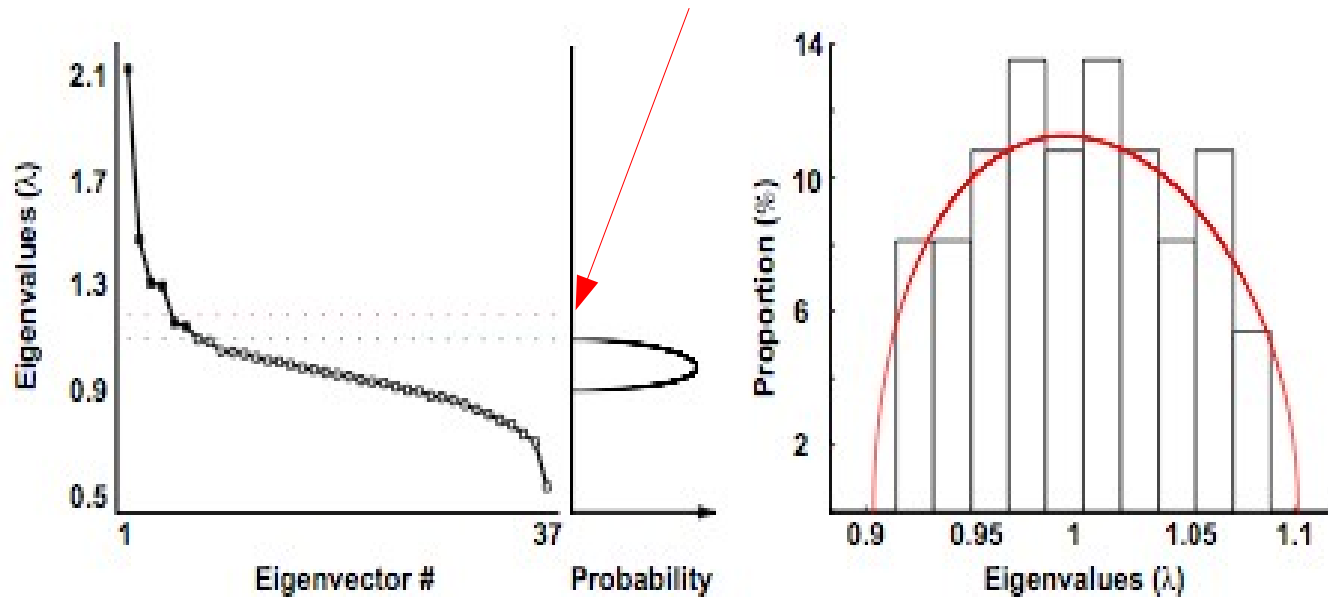
$$p_i = \frac{1}{B} \sum_{\tau=1}^B s_i^\tau$$

2. Correlation matrix computed and diagonalized

$$\chi_{ij} = \frac{p_{ij} - p_i p_j}{\sqrt{p_i p_j (1 - p_i)(1 - p_j)}}$$

3. Only eigenvectors associated to the largest eigenvalues are retained, threshold value from the upper bound of eigenvalues of correlation matrix of independent, normally distributed spike trains

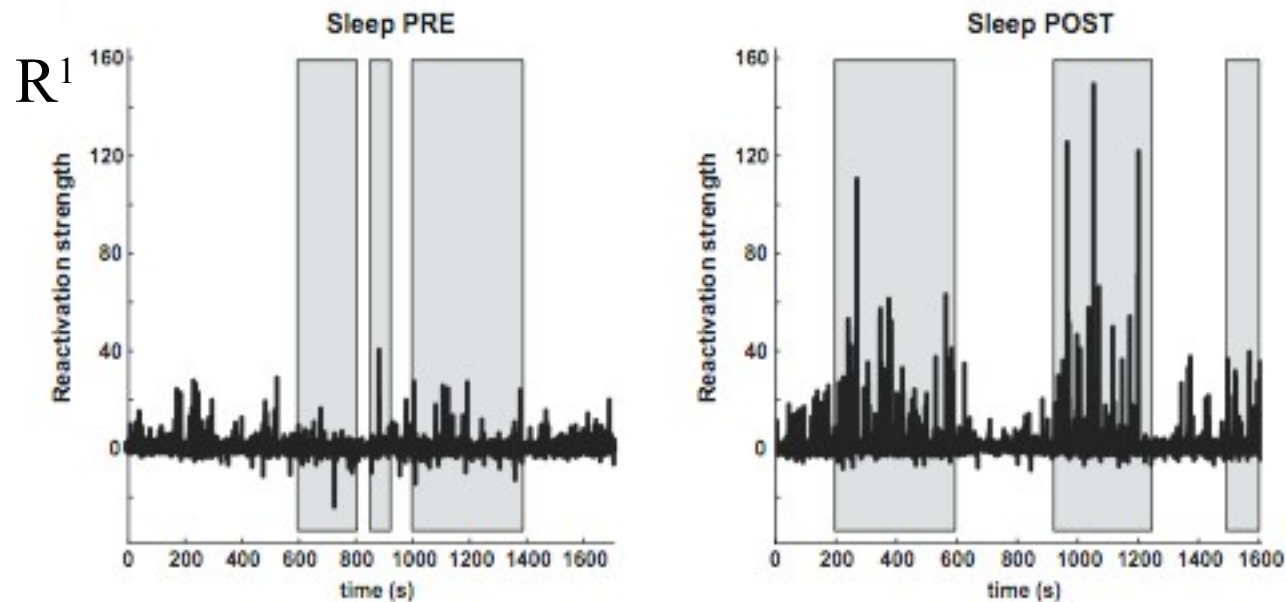
Tracy-Widom corrections



Marcenko-Pastur distribution

4. Spike trains from the sleep epoch are binned
5. The instantaneous similarity of the sleep population activity with the awake activity is computed through the

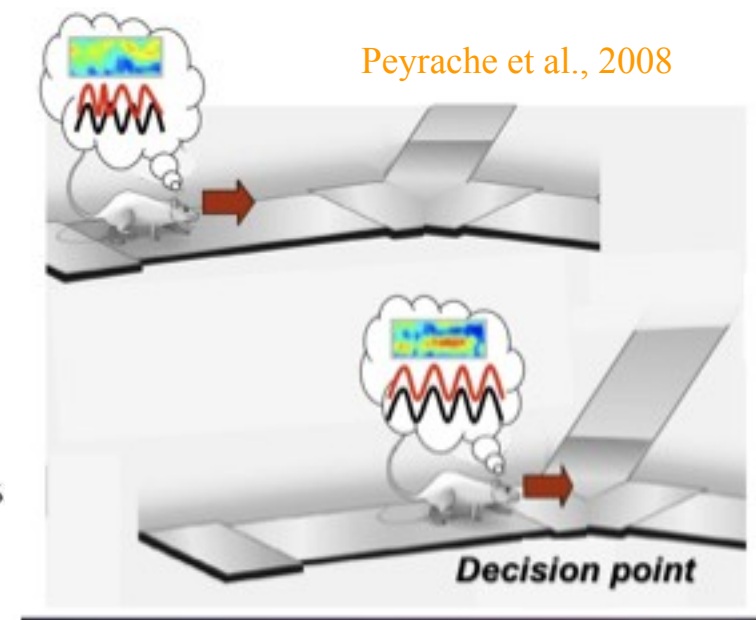
Squared overlap $R^q(\tau) = (\sum_i v_i^q s_i(t))^2$



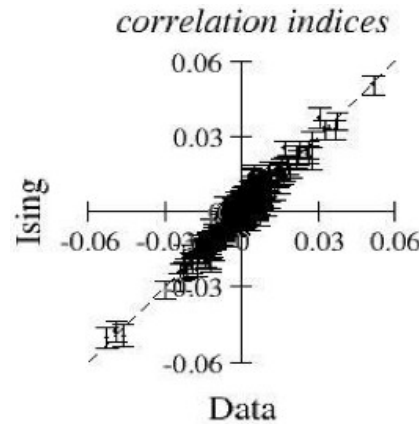
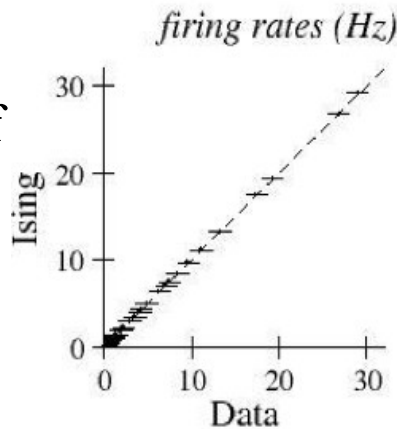
- Instantaneous similarity is high in Slow Wave Sleep (SWS) (shaded areas) after learning of the task in coincidence with hippocampal sharp waves

Analysis of the Cortical Activity of a Behaving Rat

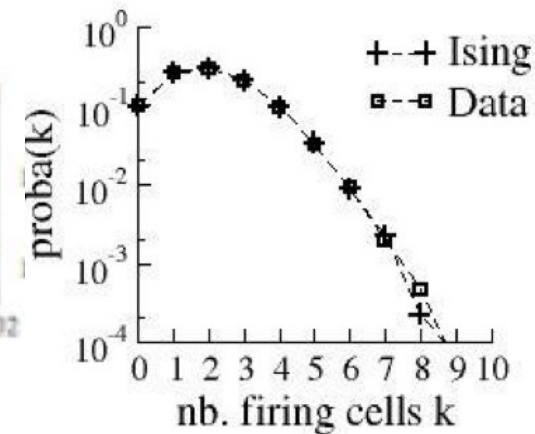
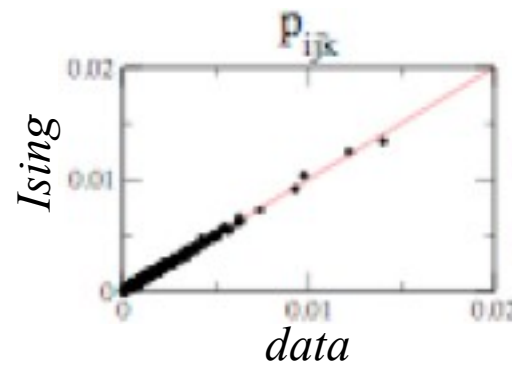
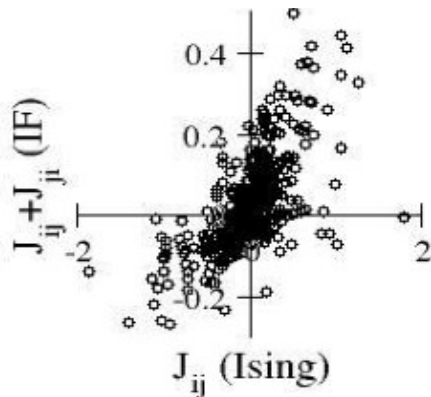
Peyrache et al., 2008



Inference of effective network J



Reproduces statistics of activity



Comparison Ising - I&F

*Exploring neural coding by novel optogenetic,
high-density microrecordings
and computational approaches*



With C. Bartic (Leuven), F. Battaglia (Amsterdam), S. Cocco (Paris), M. Giugliano (Antwerpen)

Goal 1: test capability of predicting response to a specific stimulus

Goal 2: estimate changes of network due to task learning (*distributed, sparse ?*)

Goal 3: identify & manipulate cell assemblies coding for memories